



GDR Groupement
de recherche

MI2B Outils et méthodes nucléaires
pour la lutte contre le cancer

Thème transverse Calcul

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Recent developments

- 1°) **Detector developments**
- 2°) Clinical imaging systems
- 3°) Data analysis and Python
- 4°) Complex geometry
- 5°) **AI integration**
- 6°) Multiscale simulations
- 7°) Events



CPPM Marseille

LPSC Grenoble

IP2I Lyon

LPC Clermont

IJCLab, Orsay

IPHC Strasbourg

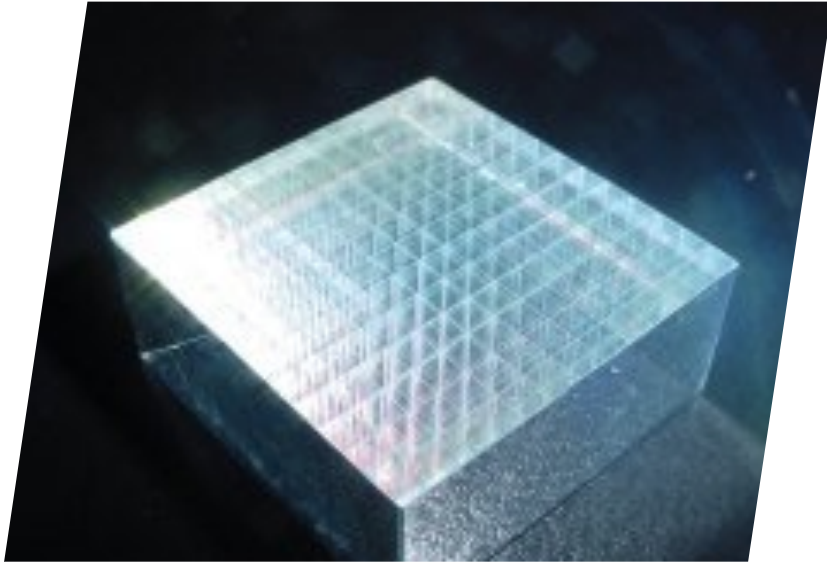
CREATIS Lyon

LATIM Brest

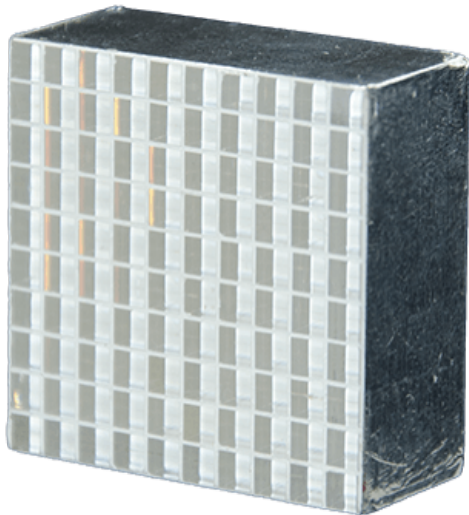
IRCM Montpellier

UC Davis

NIRS Japon



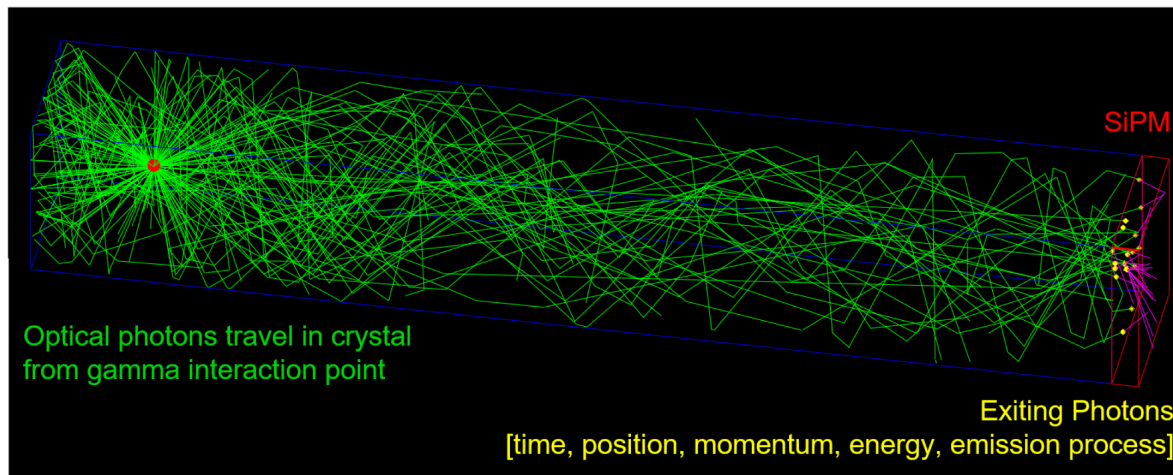
1°) Detector developments



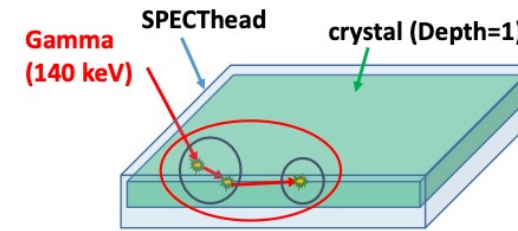
1°) Detector developments

○ 2 simulation modes

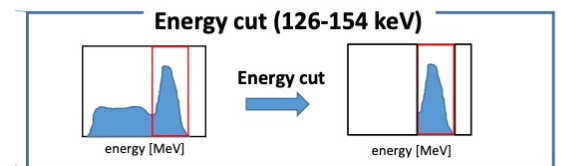
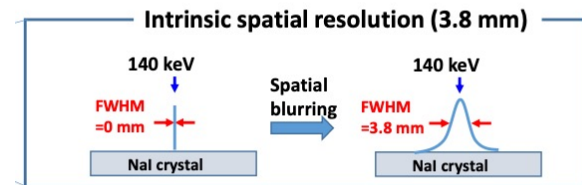
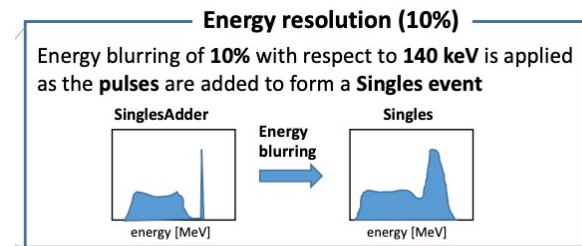
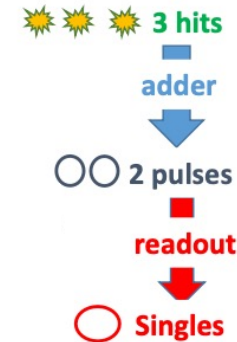
Full Monte Carlo tracking of emitted optical photons



Response of the photodetection components simulated by a specific module



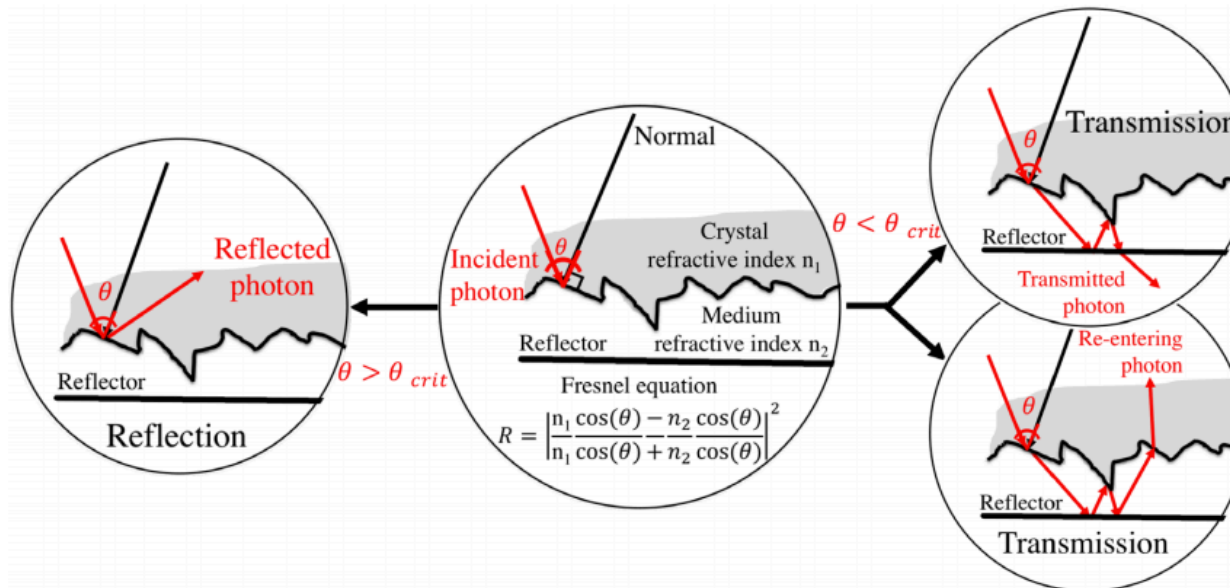
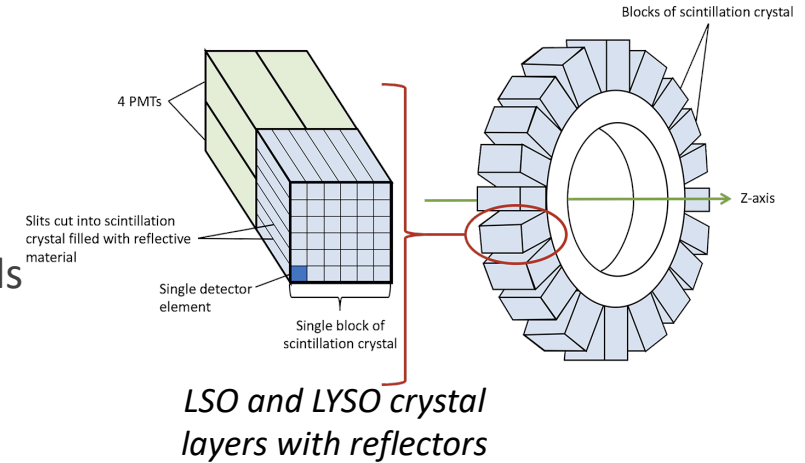
Sensitive detector



1°) Detector developments

Optical photon tracking and SiPM

- ▶ Photons many times reflected on the surface of scintillation crystal
- ▶ Process affected by specific surface treatment and reflector materials
- ▶ Manufacturing of scintillation crystals is not a standardized process
- ▶ Optical simulations based on measured crystal surfaces

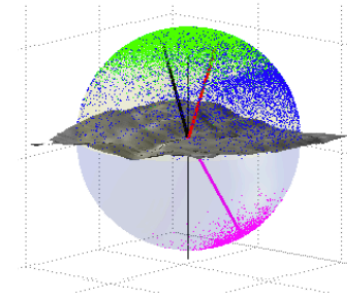
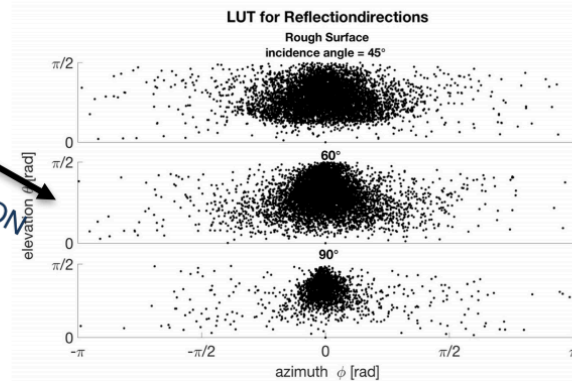
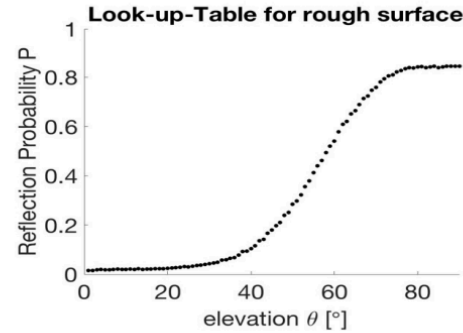
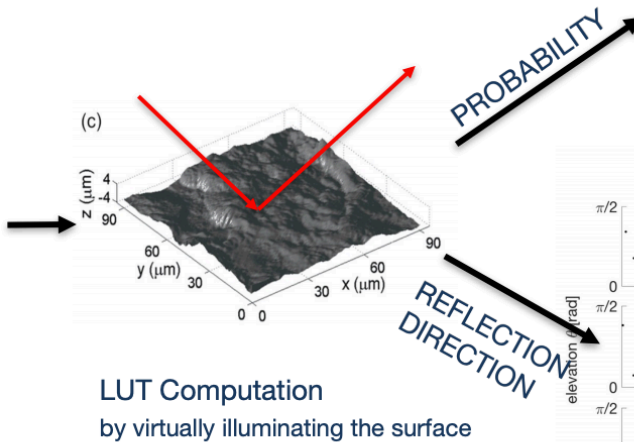
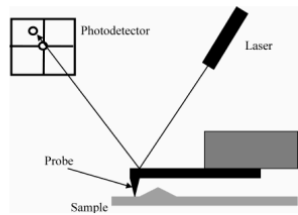


1°) Detector developments

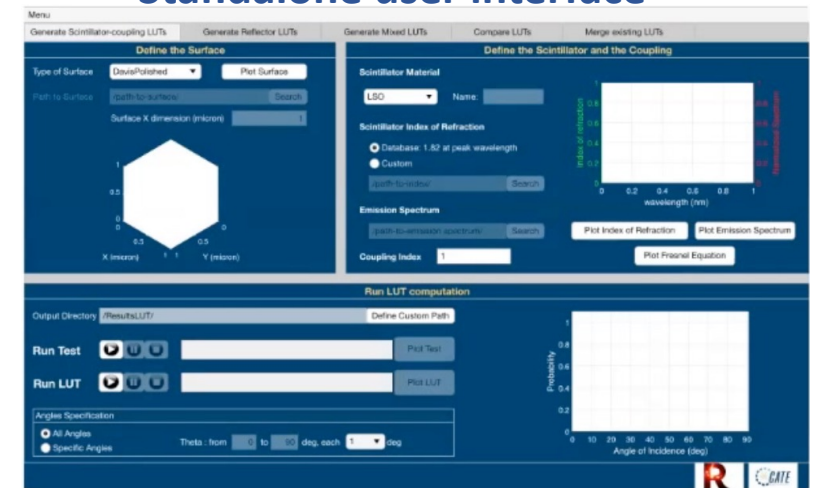
Optical photon tracking and SiPM

AFM to LUT

Atomic Force Microscopy To Look-Up-Tables



Standalone user interface



AFM measurements

LUT Computation
by virtually illuminating the surface

► Integrating reflector and surface finish

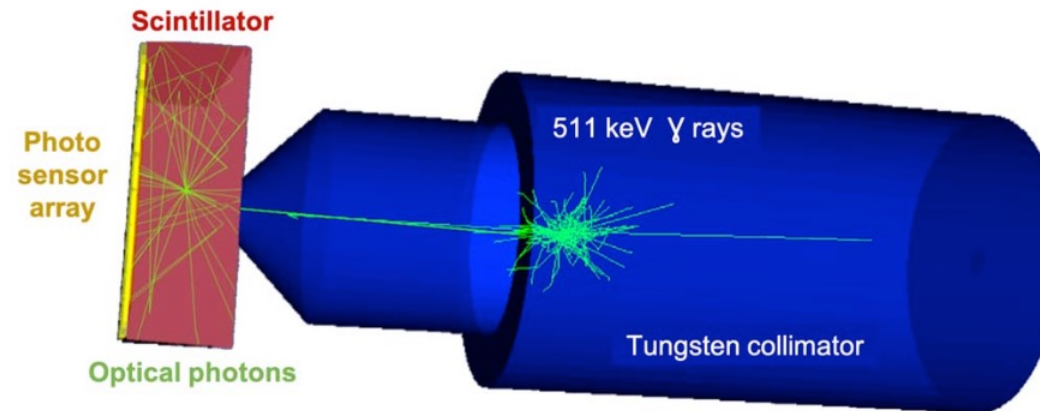
- Reflectors: ESR, Teflon
- Coupling: Air, optical grease
- Surface finish: Polished, Rough

Trigila C, Moghe E and Roncali E 2021 Standalone application to generate custom reflectance Look-Up Table for advanced optical Monte Carlo simulation in GATE/Geant4 Med Phys.

1°) Detector developments

Optical photon tracking and SiPM

- Large monolithic scintillation detector for clinical PET systems

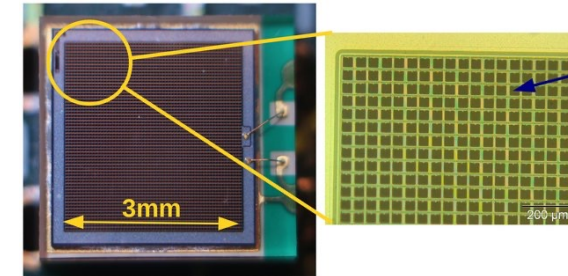


- gain insight into
 - physical processes difficult or impossible to measure experimentally, especially DOI.
 - influence of Compton scattered events,
 - influence of intrinsic ^{176}Lu radiation of the scintillator,
 - influence of test-equipment, e.g. collimators or housing.

1°) Detector developments

Optical photon tracking and SiPM

- Increasing use of SiPM in PET imaging
 - Specific digitizer modules for analog (aSiPM) and digital SiPMs (dSiPM)

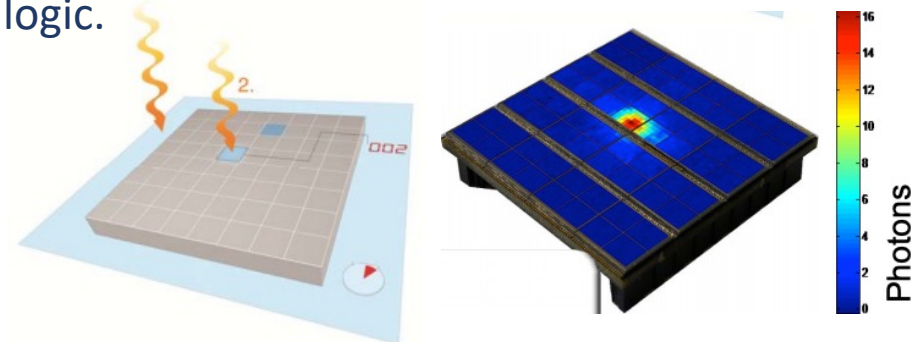
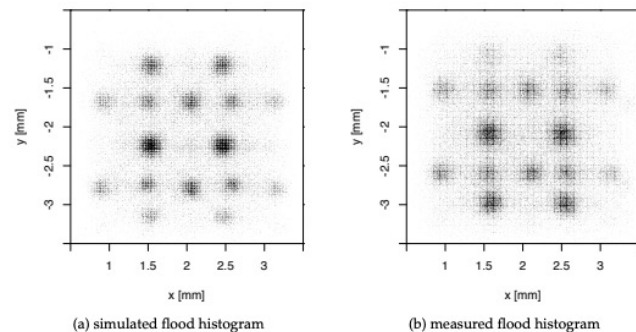


- aSiPM: takes into account aSiPM saturation and various sources of noise such as dark counts, crosstalks, afterpulses, after-crosstalks and signal white noise

Mehadji B 2020 Modélisation Monte Carlo d'une caméra Compton basée sur l'utilisation de détecteurs à scintillation sensibles à la position couplés à des SiPM PhD Thesis Aix-Marseille Université J. Instrum.

- dSiPM: (Philips Digital Photon Counter)

- takes into account noise sources (dark noise and optical crosstalk), the PDE of the sensor, and the specific trigger and validation logic.



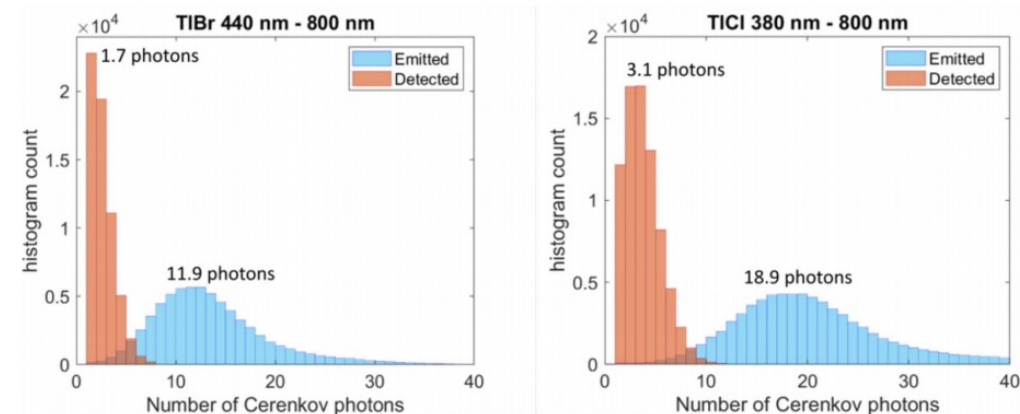
*Lenz M 2020 Design and characterisation of an MRI compatible human brain PET insert by means of simulation and experimental studies
PhD Thesis Bergische Universität Wuppertal*

1°) Detector developments

Cerenkov-based TOF

- use of ultra-fast (10 ps) Cerenkov emission for TOF PET detectors = alternative to traditional time triggering on scintillation photons
- very low number of Cerenkov photons produced by each gamma interaction in the Cerenkov radiator (around 15–20 per photoelectric interaction for BGO)
- Cerenkov production and transport in the crystal
 - direction of the initial Cerenkov photons,
 - contribution of Cerenkov photons to the detector timing resolution.

Ariño-Estrada G, Roncali E, Selfridge A R, Du J, Glodo J, Shah K S and Cherry S R 2020 Study of Čerenkov light emission in the semiconductors TlBr and TlCl for TOF-PET IEEE Trans. Rad. Plasma Med. Sci. 1



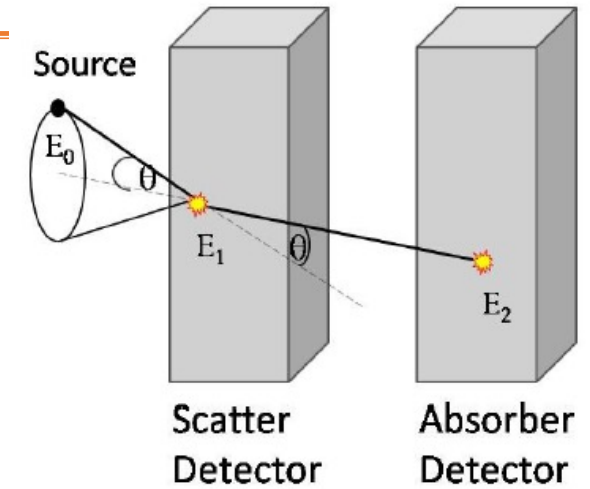
For 75000 photoelectric events

1°) Detector developments

Compton camera modules

○ Principle

- Classic gamma camera:
 - inverse proportionality relationship between sensitivity and spatial resolution
 - Collimator thickness to be adjusted to the gamma energy
- Compton Camera
 - Electronic collimation: at least 2 detectors
 - Compton scattering in the 1st detector (scatterer)
 - Photoelectric absorption in the 2nd detector (absorber)
 - Calculation of the scattering angle of the Compton interaction
 - Reconstruction of a cone with the source position located on cone surface
 - Intersection of the cones calculated for different gammas emitted from the source lead to the definition of the source position



$$\cos(\theta) = 1 - \frac{E_1 m_e c^2}{E_0 (E_0 - E_1)}$$

○ Challenges

- Higher efficiency: every gamma photon reaching the camera has a probability to be scattered
- Image resolution depends only on detectors involved
- Wider range of gamma energies
- Reconstruction through cone:=> 3D activity map obtained without moving the camera

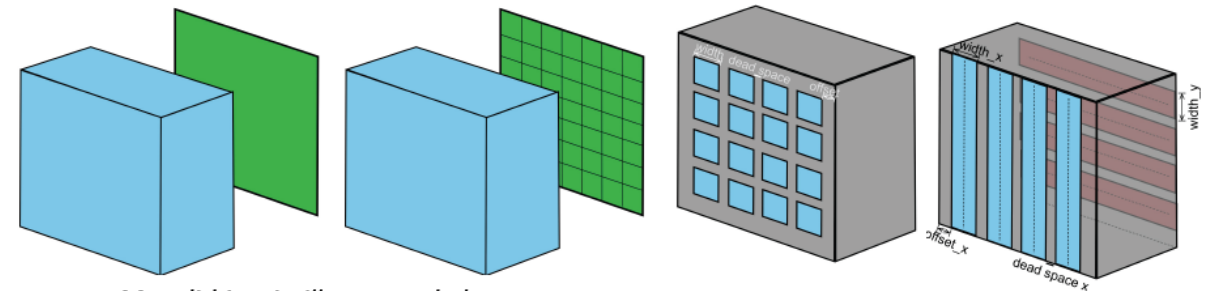
1°) Detector developments

Compton camera modules

MC framework adapted to different detector geometry

- ▶ Design, optimize and predict the potentiality of the system
- ▶ Understand experimental data
- ▶ Study background rejection techniques
- ▶ Test reconstruction algorithms

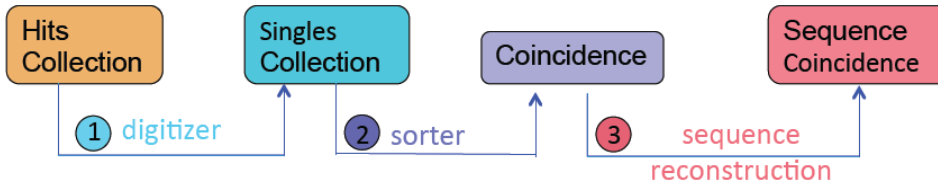
CCMod: a GATE module for Compton camera imaging simulation - <https://doi.org/10.1088/1361-6560/ab6529>



Monolithic scintillator coupled to position sensitive/insensitive detector

Pixelated crystals

Strip detectors

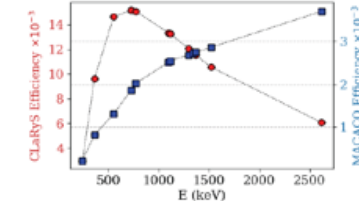


- 1 A chain of digitizer modules applied to the different detector layers to model the detector response or to recover ideal Compton kinematics
- 2 Time coincidence between the pulses in the different layers
- 3 Sequence reconstruction: order singles within a coincidence

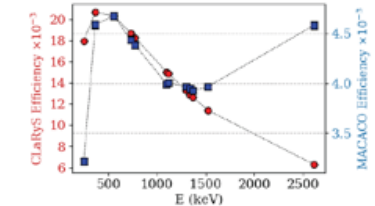
Output data available at each step
 Processing steps (1,2,3) may be performed on-the-fly or offline
 Same data structure as for PET/SPECT sys to be able to share developed processors

Detection efficiency normalized to the scatterer geometrical efficiency

CLaRyS: $THR_{scatt}=50$ keV, $THR_{abs}=100$ keV
 MACACO: 85 keV

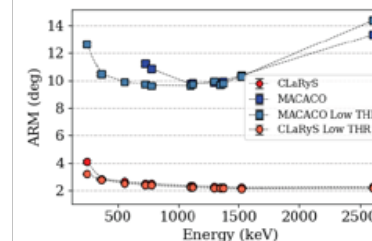


THR: 10 keV for both systems



Only 2-single-coincidences are considered

Angular Resolution measure



Energy Resolution in the scatterer

MACACO: 8.5% @ 511 keV
 CLaRyS: 1.56% @ 511 keV

X-Y spatial resolution

MACACO: 2 mm sigma
 CLaRyS: 0.4 mm sigma
 (assuming normal distribution in the 1.4 mm strip)

2°) Clinical imaging systems

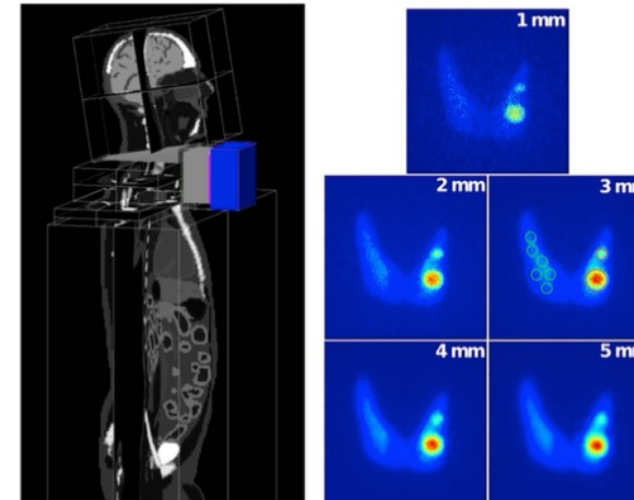
Simulated cameras for 10 years

Preclinical and clinical PET systems

2011 McIntosh <i>et al</i> (2011)	PC	Inveon, LSO, by Siemens
2011 Geramifar <i>et al</i> (2011)	C	Discovery RX, LYSO, by GE
2012 Poon <i>et al</i> (2012)	C	Biograph mCT, LSO, by Siemens
2012 Trindade <i>et al</i> (2012)	C	Gemini TF, TruFlight Select, LYSO, by Philips
2013 Lee <i>et al</i> (2013)	PC	Inveon trimodal, LSO, by Siemens
2013 Nikolopoulos <i>et al</i> (2013)	PC	Biograph DUO, LSO, by Siemens
2013 Zagni <i>et al</i> (2013)	PC	Argus, LYSO/GSO, DOI, by Sedecal
2013 Solevi <i>et al</i> (2013)	C	prototype AX-PET, LYSO, SiPM, brain
2015 Moraes <i>et al</i> (2015)	C	Biograph mCT, LSO, by Siemens
2015 Poon <i>et al</i> (2015)	C	Biograph mCT, LSO, by Siemens
2015 Aklan <i>et al</i> (2015)	C	Biograph mMR hybrid, LSO, by Siemens
2015 Monnier <i>et al</i> (2015)	C	Biograph mMR hybrid, LSO, by Siemens
2016 Lu <i>et al</i> (2016)	PC	Inveon, LSO, by Siemens
2016 Etxebeste <i>et al</i> (2016)	PC	prototype, LYSO
2017 Shekhzadeh <i>et al</i> (2017)	C	NeuroPET, LYSO, SiPM, brain, by PDS
2017 Li <i>et al</i> (2017)	C	Ray-Scan 64, BGO, by ARRAYS MIC
2018 Del Guerra <i>et al</i> (2018)	C	prototype TRIMAGE, LYSO
2018 Kowalski <i>et al</i> (2018)	C	prototype J-PET, plastic
2019 Abi Akl <i>et al</i> (2019)	C	prototype PET2020, LYSO
2019 Kochebina <i>et al</i> (2019)	C	prototype CaLIPSO, TMBi
2020 Emami <i>et al</i> (2020)	C	Dual ring MAMMI breast, LYSO, by Oncovision
2020 Salvadori (2020)	C	Vereos, LYSO, SiPM, Philips

Preclinical and clinical SPECT systems

2010 Mok (2010)	PC	XSPECT, multi-pinhole, ^{99m}Tc , by Gamma Medica-Ideas
2011 Robert <i>et al</i> (2011)	C	prototype, HiSens, CZT, LEHR/H13, ^{99m}Tc , ^{57}Co
2011 Boisson <i>et al</i> (2011)	PC	prototype, parallel slat, YAP:Ce, ^{99m}Tc , ^{57}Co
2015 Lee <i>et al</i> (2015b)	PC	Symbia T2, LEAP/LEHR/HE, ^{131}I , ^{99m}Tc , by Siemens
2015 Lee <i>et al</i> (2015a)	PC	Inveon, LSO, ^{123}I , ^{125}I , by Siemens
2015 Spirou <i>et al</i> (2015)	C	ECAM, NaI(Tl), ^{99m}Tc , by Siemens
2017 Georgiou <i>et al</i> (2017)	PC	γ -eye, CsI(Na), ^{99m}Tc , ^{111}In , ^{177}Lu , by Bioemtech
2017 Costa <i>et al</i> (2017)	C	Symbia T2, MEAP, ^{177}Lu , by Siemens
2018 Taherparvar and Sadremomtaz (2018)	PC	prototype, CsI(Na), ^{99m}Tc
2019 Sadremomtaz and Telikani (2019)	PC	HiReSPECT, LEHR, CsI(Na), ^{99m}Tc , by PNP



THIDOS compact mobile γ -camera for absorbed radiation dose control in IRT.

Trigila C 2019 Development of a portable gamma imaging system for absorbed radiation dose control in molecular radiotherapy PhD Thesis, Université Paris-Saclay (<https://tel.archives-ouvertes.fr/tel-02475983/document>)

3°) Data analysis and Python

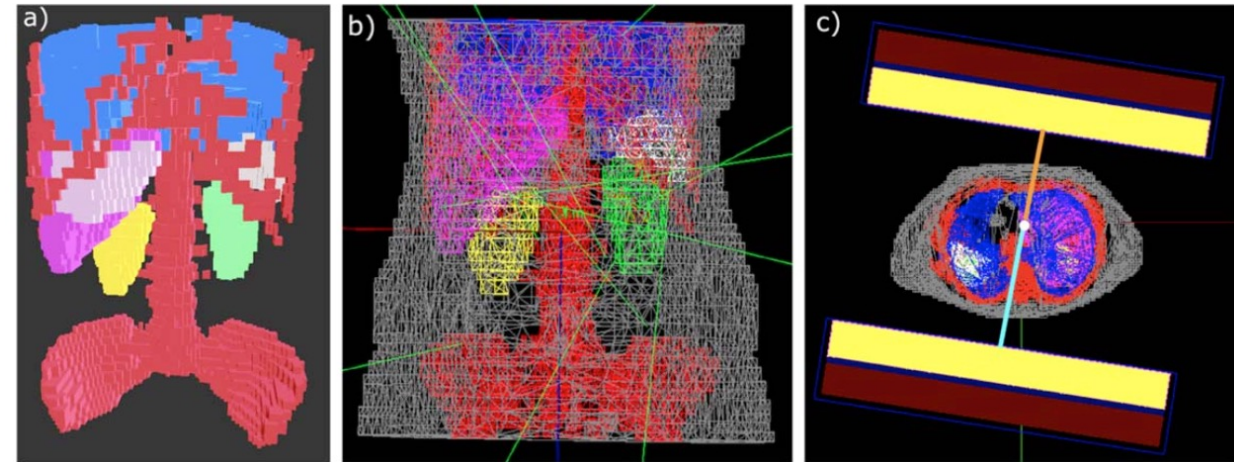


<https://github.com/OpenGATE/GateTools>

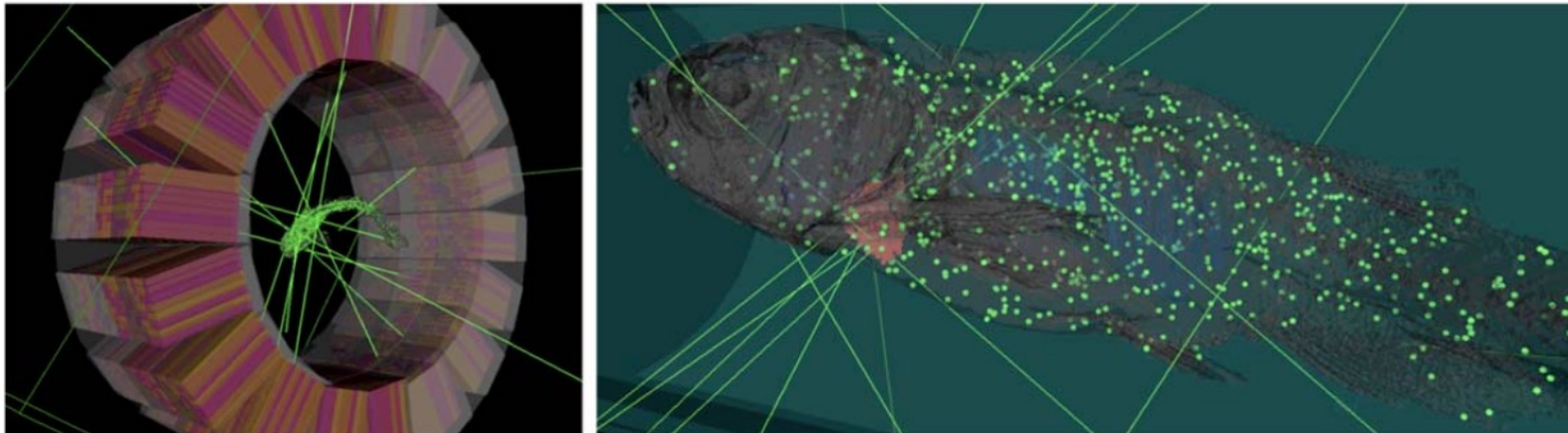
- Python: easy to learn & easy to use
 - NumPy, Matplotlib, uproot...
 - read/write data in NPY file format
- Opensource set of tools
 - convert or resize images in various file formats,
 - convert DICOM RT structures,
 - manage phase-space files
 - analyze dose map, with DVH (Dose Volume Histogram) or gamma-index for example.
- To a long term development
 - Python wrapping : pybind11

4°) Complex geometries

- Tessellated mesh geometries
 - STL files
 - Auto-contouring SPECT gamma cam motion
 - Used for attenuation and emission phantoms



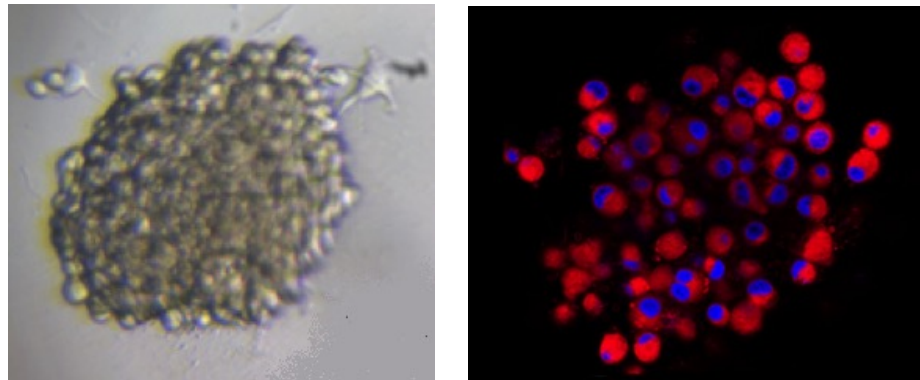
Kayal G, Chauvin M, Mora-Ramirez E, Struelens L and Bardies M 2020b Implementation of SPECT auto-contouring detector motion in GATE Monte Carlo simulation for ^{177}Lu and ^{131}I molecular radiotherapy (MRT) dosimetry *Eur J Nucl Med Mol Imaging* 47 1–753



Zvolský M, Schreiner N, Seeger S, Schaar M, Rakers S and Rafecas M 2019a Digital zebrafish phantom based on micro-CT data for imaging research *IEEE Nuc. Sci. Symp. and Med. Imaging Conf.(NSS/MIC)* 2019 1–2

4°) Complex geometries

○ Tessellated mesh cell populations



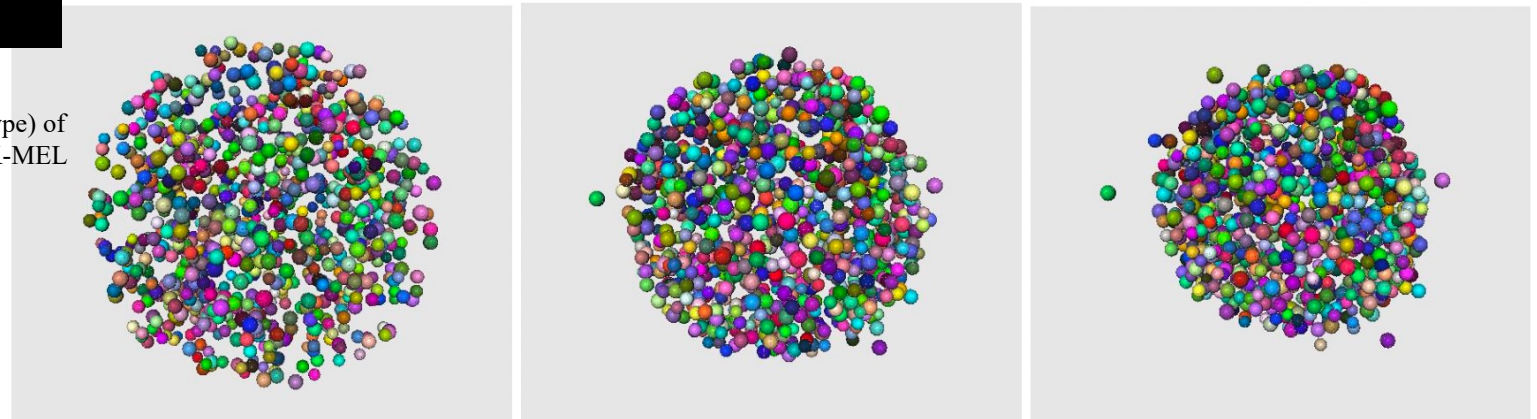
(a)

(b)

Figure 1. (a) Reverse-phased microscopy imaging of a spheroid (SK-MEL 28 type) of $550 \pm 40 \mu\text{m}$ in diameter (b) Fluorescent confocal microscopy of a spheroid (SK-MEL 28 type)

- model large three-dimensional cell populations
- independent deformable cells described with their nucleus, cytoplasm and membranes
- force law systems to manage cell-cell interactions.

CPOP: An open source C++ cell POPulation modeler for radiation biology applications, L. Maigne, A. Delsol, G. Fois, E. Debiton, F. Degoul, H. Payno, August 02, 2021, DOI:<https://doi.org/10.1016/j.ejmp.2021.07.016>

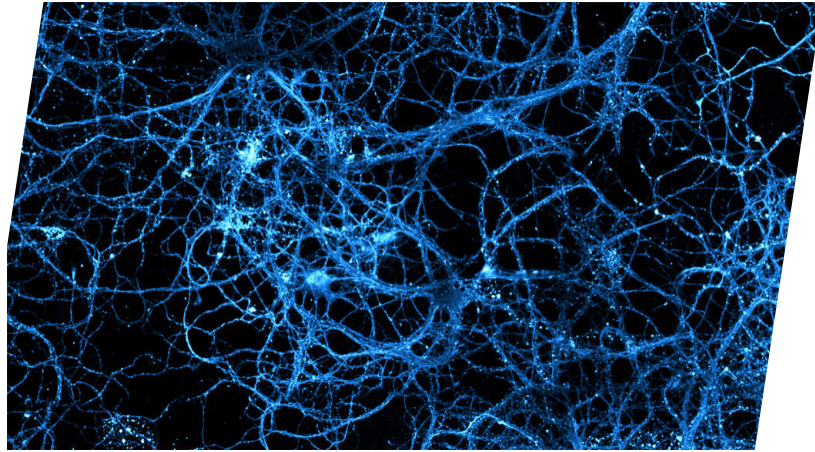


(a)

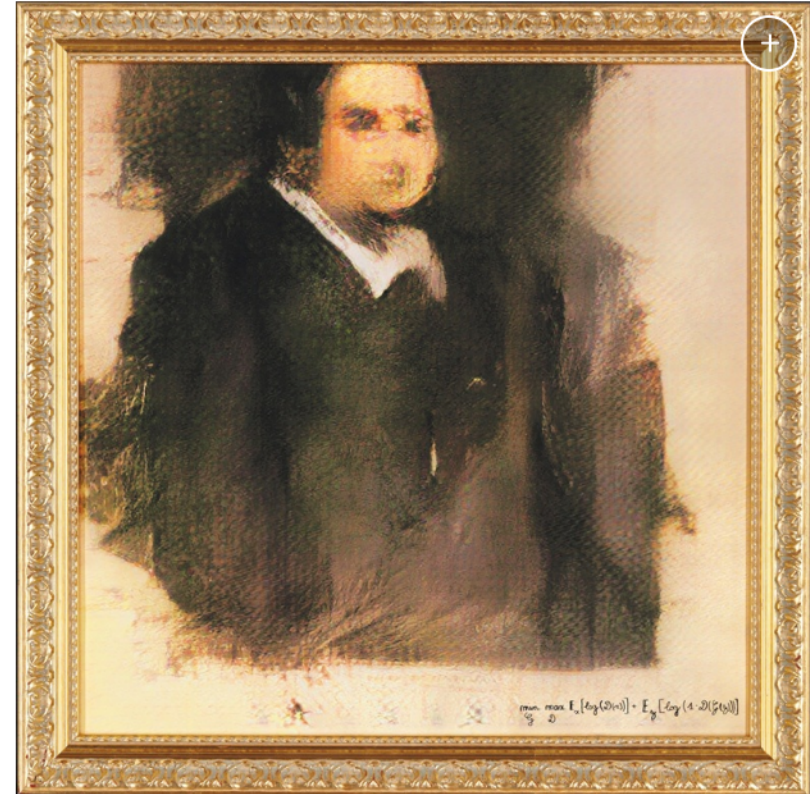
(b)

(c)

Figure 9. Spheroids corresponding to SK-MEL28 cell populations. (a) 962 cells generated without forces (defined as 3DCellPopulation.xml in the following studies), (b) 989 cells generated with a force rigidity=0.0007, (c) 989 cells generated with a force rigidity=0.002.



Artificial Neural Networks (ANN)

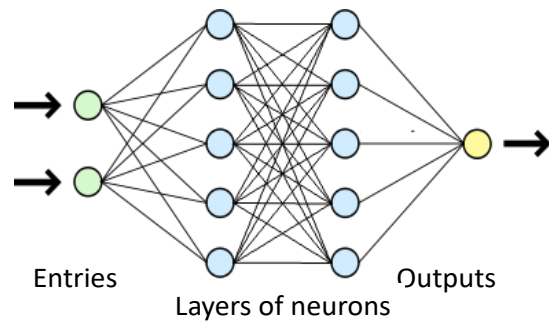


Portrait of Edmond Belamy, 2018, created by GAN (Generative Adversarial Network). Sold for \$432,500 on 25 October at Christie's in New York. Image © Obvious

Generative Adversarial Networks (GAN)

5°) AI integration (MC)

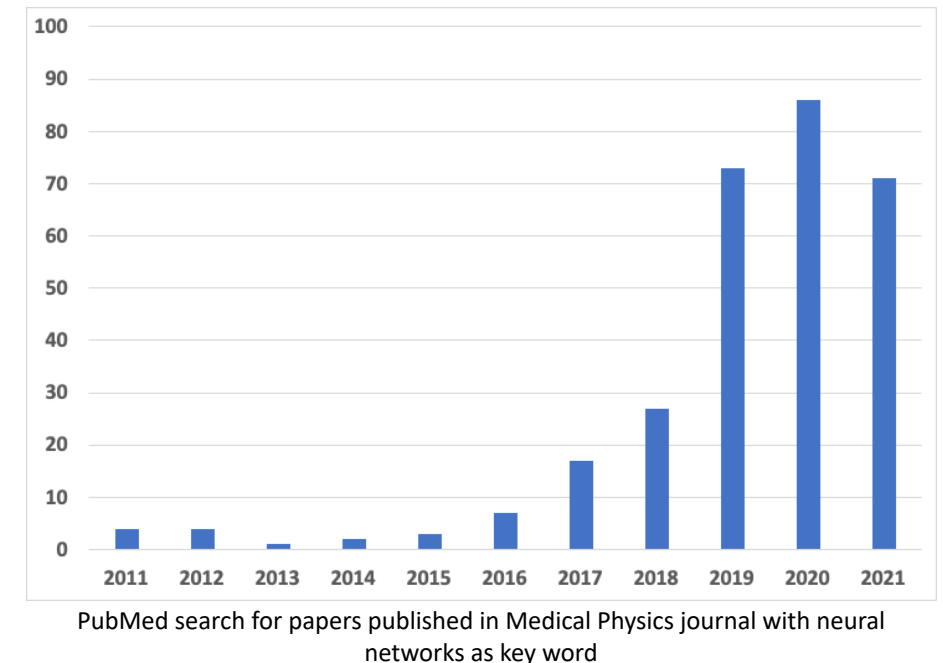
- Monte Carlo simulations can **produce** highly accurate imaging device and patient training datasets for neural networks



Neurons: one weight per neuron

Layer: linear combination + activation function (non-linear)

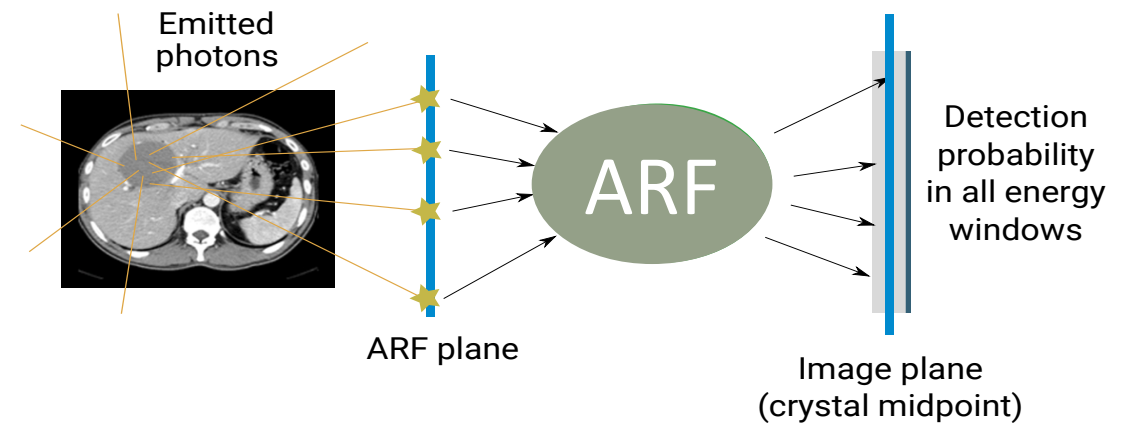
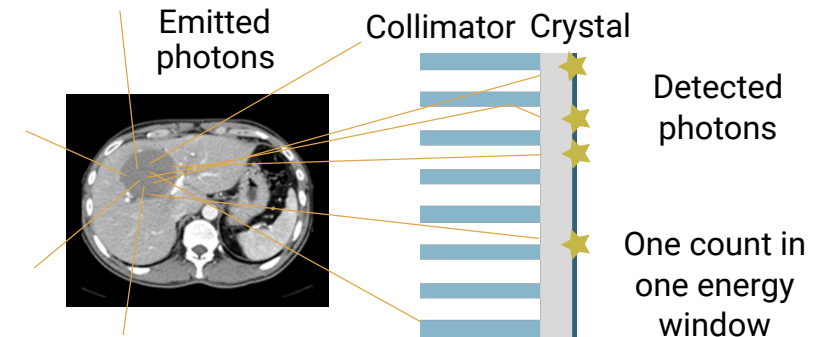
- deep learning approaches can be **applied** to improve Monte Carlo simulation performance (computational efficiency)



5°) AI integration (MC)

SPECT imaging and ARF function

- ▶ Accelerate computing time for the simulation of interactions in the head of the camera
 - ▶ Only few photons are reaching the detection
- ▶ Several Variance Reduction Techniques proposed
- ▶ Angular Response Function (ARF)
 - ▶ Replace SPECT head detection with tabulated response
 - ▶ Incident particle at ARF plane use tables to get energy windows probabilities
- ▶ Assume:
 - ▶ Spatially invariant
 - ▶ Detection depends on direction + energy
- ▶ Speedup factor between 20 and 100
- ▶ Computed only once



Sarrut et al. Learning SPECT detector angular response function with neural network for accelerating Monte-Carlo simulations, *Phys. Med. Biol.* 2018
<https://doi.org/10.1088/1361-6560/aae331>

5°) AI integration (MC)

SPECT imaging, GAN and ARF-nn function

- (1) generate the training dataset via Monte Carlo simulation,
- (2) train the GAN
- (3) use the generator of the GAN as a source.
- (4) a second neural network (ARF-nn), is used to model the imaging detector response and the two neural networks are combined.

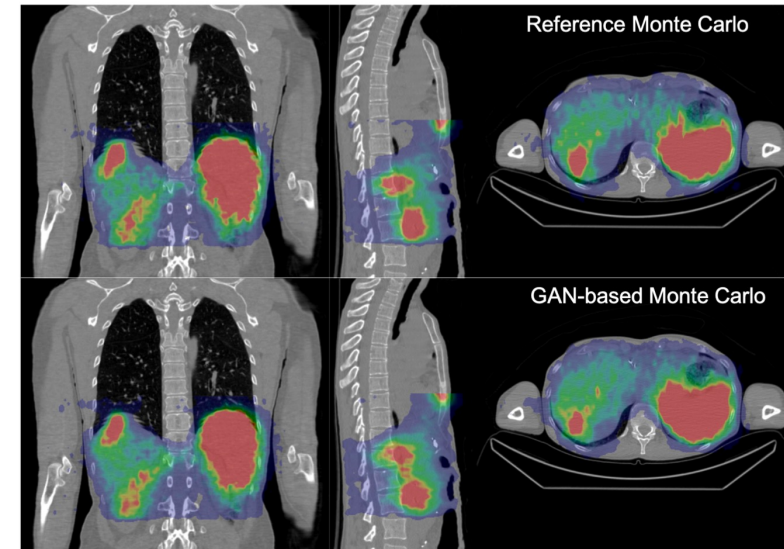
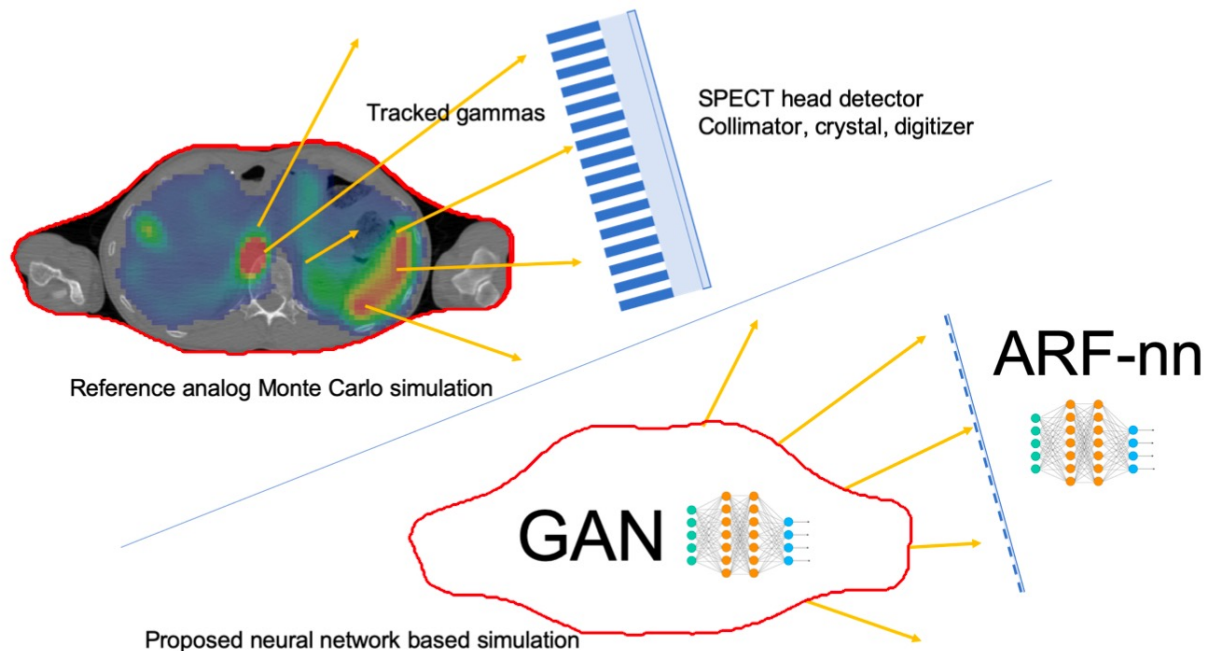


Figure 10. Reconstructed tomography SPECT overlaid on patient CT slides. Upper row: reconstruction performed with the projections obtained from the reference simulation plus ARF-nn; lower row: projections obtained via the combined GAN/ARF-nn method.

Sarrut, D., Etxebeste, A., Krah, N., Létang, J.M.
 Modeling complex particles phase space with GAN for Monte Carlo SPECT simulations: a proof of concept. *Phys Med Biol* 66, 055014, 2021

5°) AI integration (MC)

Application to the generation of PHSP files

1 – Generate training dataset (PHSP)

2 – Train GAN

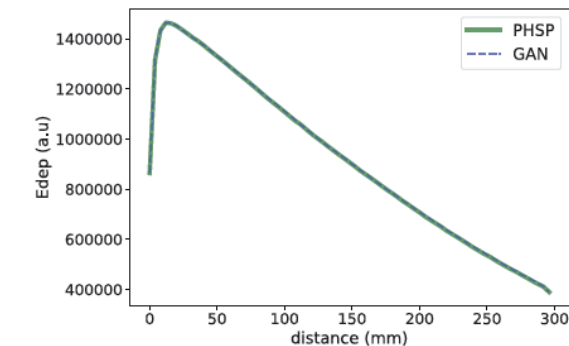
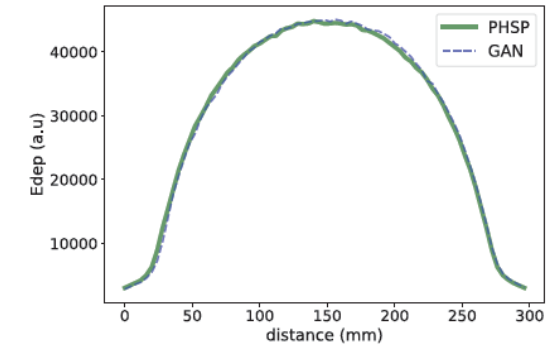
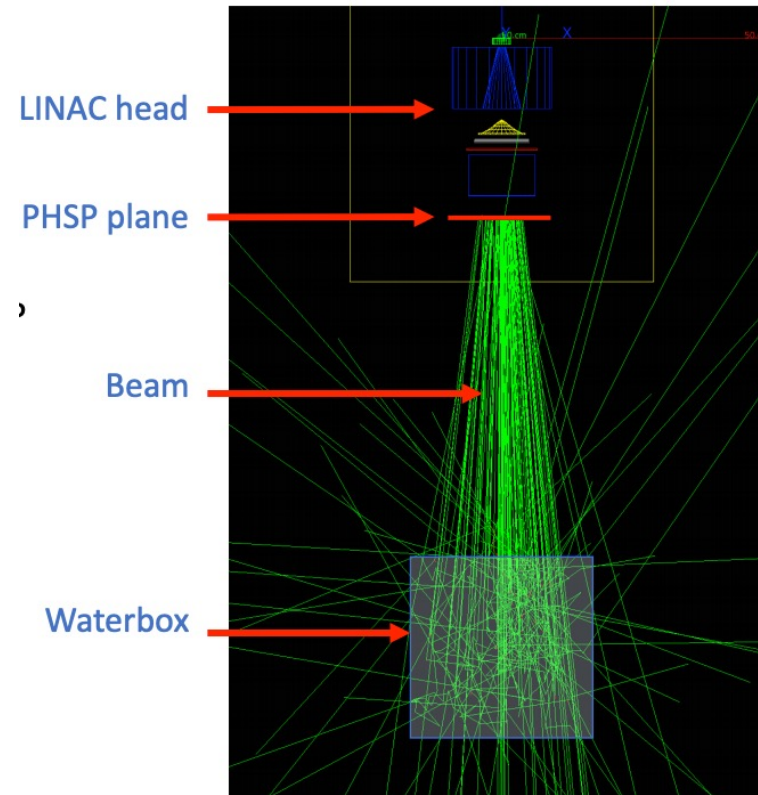
3 – Generate PHSP from GAN

4 – Use PHSP to compute dose in waterbox

5 – Compare

Sarrut et al. Generative Adversarial Networks (GAN) for compact beam source modelling in Monte Carlo Simulations, Med. Phys., doi: 10.1088/1361-6560/ab3fc1

PHSP	Size	Nb of particles
Elekta PRECISE 6MV	2 files of 3.9 GB	1.3×10^8 photons each file
CyberKnife IRIS 60mm	2 files of 1.6 GB	5.8×10^7 photons each file



5°) AI integration (MC)

MoCaMed: Advanced Monte Carlo Methods for Medical Physics



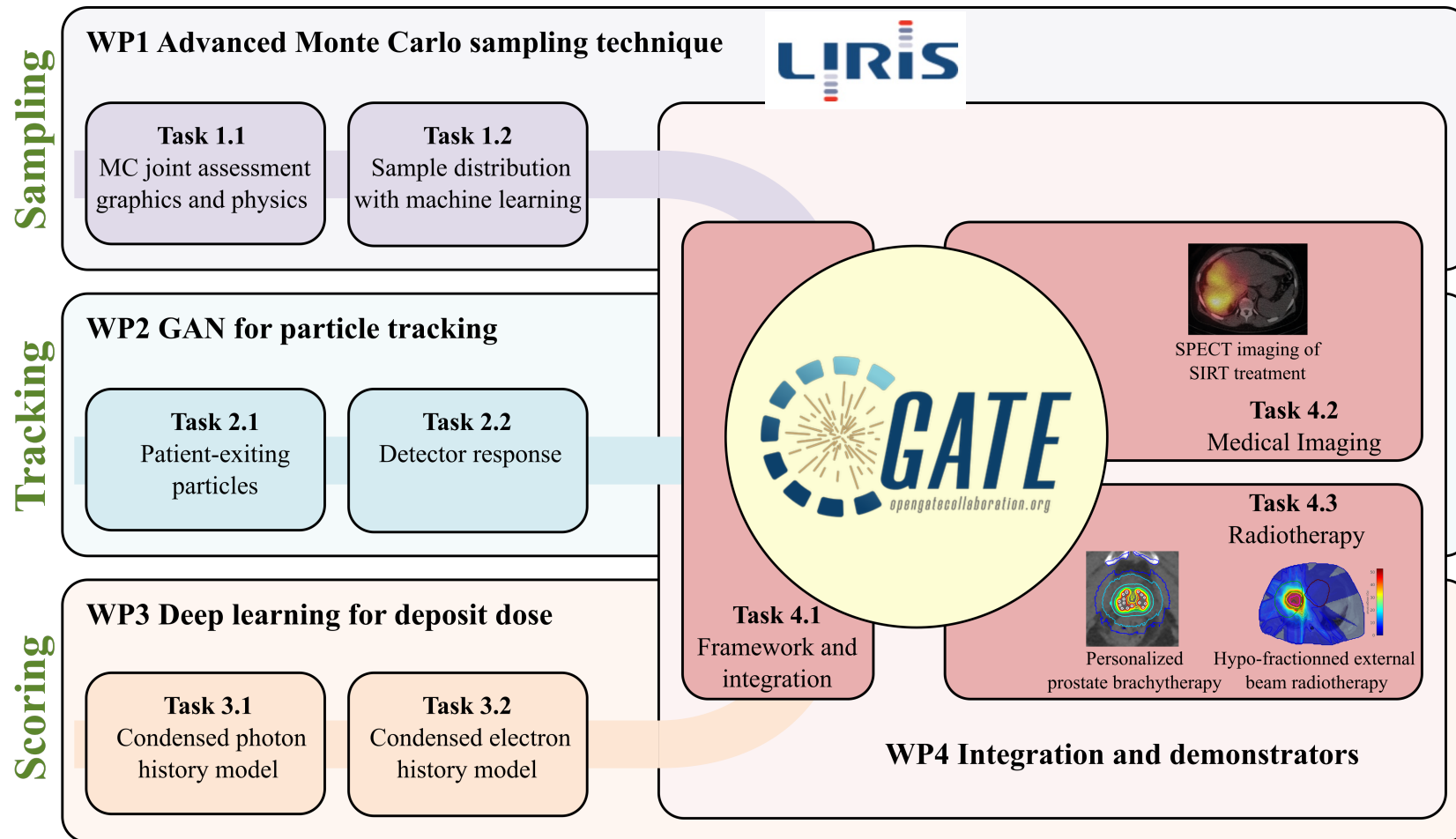
CREATIS

ANR AAPG2020 – CE45

42 months

Partners

- LaTIM (INSERM), Julien Bert
- CREATIS (CNRS, INSERM), Ane Etxebeste, David Sarrut
- LIRIS (CNRS), David Coeurjolly, Nicolas Bonneel, Julie Digne, Victor Ostromoukhov



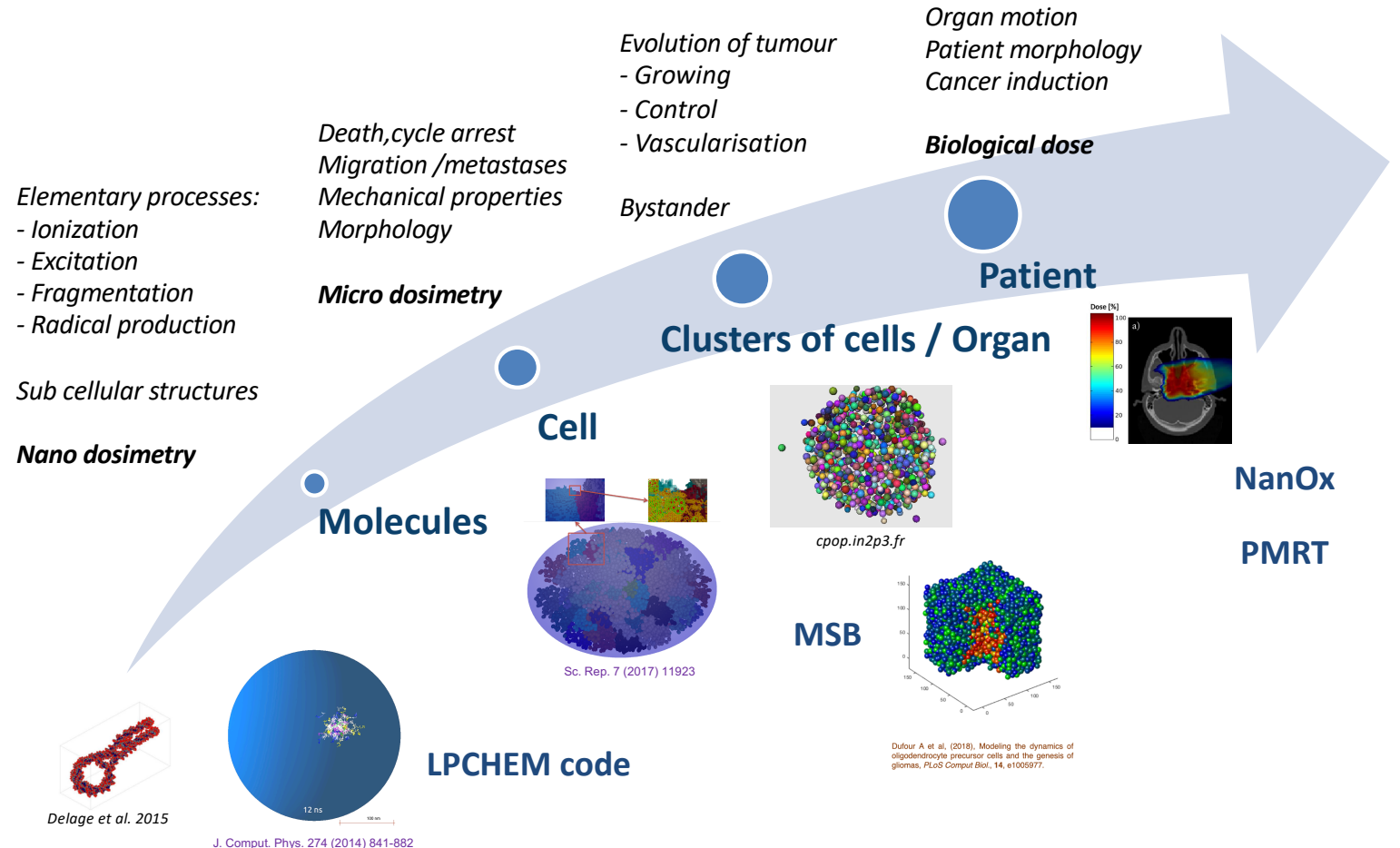
6°) Multiscale simulations



The **unique** open source and open access simulation toolkit for micro/nano dosimetry and radiation biology

- **Long term development** fully included in Geant4 releases
- International collaboration composed of 42 collaborators
- **Coordinated by IN2P3/CNRS** since 2008
- Funded by regular support from institutions and international calls
- Fruitful involvement in international conferences & tutorials
 - Geant4 International User Conference at the Physics-Medicine-Biology frontier » series of conferences initiated by IN2P3 in 2005
 - Annual international tutorials (17)
- High rank and highly cited publications (104 since 2007)

DEVELOPMENT ACCESSIBLE TO OTHER TOOLKITS, PARTICULARLY TO GATE



Open source and open access toolkits

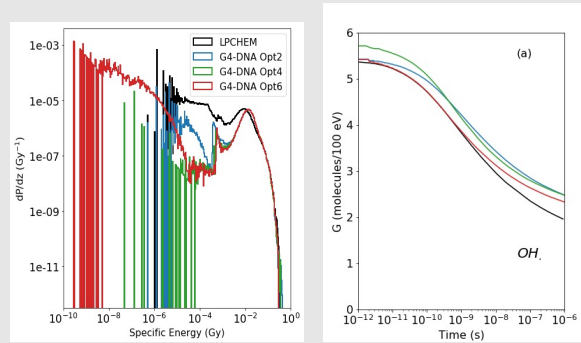


6°) Multiscale simulations

Evaluation of the biological dose in hadrontherapy

BIOPHYSICS MODELS

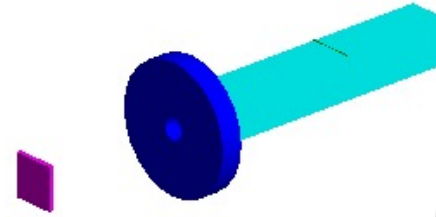
PRE CALCULATED DATA WITH TRACK STRUCTURE MC CODES



Evaluation of alpha and beta parameters for mono-energetic ion beams using data such as specific energy and water radiolysis

CLINICAL BEAM MODELING

HIMAC BEAM LINE GEOMETRY IN GATE



BIODOSE ACTOR

The biodose actor uses the biophysics models predictions to calculate the biological quantities for an SOBP in a voxelized target

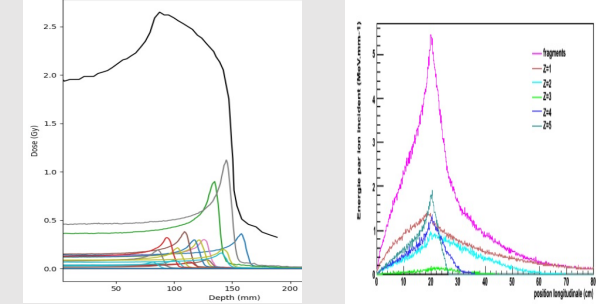
RBE

BIOLOGICAL DOSE

SURVIVAL FRACTION

SOBP

IRRADIATION FIELD WITH PRIMARY IONS AND NUCLEAR FRAGMENTS OF DIFFERENT LET



The physical dose deposition is simulated for the clinical beam line as an SOBP using PBS or passive modulation

Thèse LabEx PRIMES

Yasmine ALI (soutenance décembre 2021)

6°) Multiscale simulations

Biophysical models

MMKM

Kase et al. (2006)
Inaniwa T. et al. (2010)



BIOLOGICAL DATA

REFERENCE EXPERIMENTAL DATA

Reference α , β values, cell nucleus
and radius of the sensitive volume



PHYSICAL DATA

PRECALCULATED WITH TSMC (G4DNA, LQD)

Specific energy deposited in the cell sensitive
volume on a micro and nanometric scale



CHEMICAL DATA

PRECALCULATED WITH TSMC (G4DNA, LQD)

Yield of radiolytic species in the sensitive volume

NANOX

Cunha et al. (2017)
Monini et al. (2020)

6°) Multiscale simulations

Estimate cell survival

data/V79_NanOx.txt

data/CHO-K1_NanOx.txt

data/SQ20B_NanOx.txt

data/HSG_NanOx.txt

KINETIC ENERGY (MeV/n)	α	β
Hydrogen ion		
0.1	3.52	0.05
0.125	3.58	0.02
Helium ion		
0.1	1.35	0.02
0.125	1.34	0.01
Carbon ion		
0.1	0.55	0.01
0.125	0.20	0.03
Oxygen ion		
0.1	0.41	0.01
0.125	0.38	0.02

data/HSG_MMKM.txt

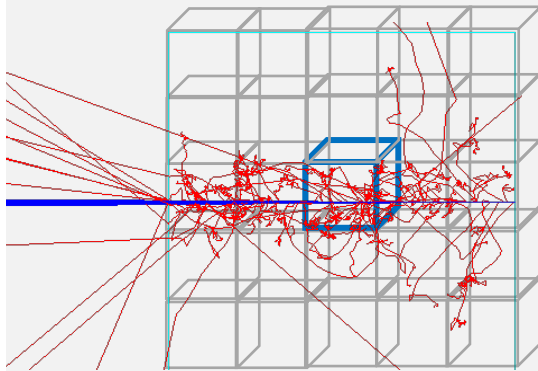
KINETIC ENERGY (MeV/n)	α	β
Hydrogen ion		
0.1	1.57	0.047
0.125	1.54	0.047
Helium ion		
0.1	1.24	0.047
0.125	1.22	0.047
Carbon ion		
0.1	0.46	0.047
0.125	0.45	0.047
Oxygen ion		
0.1	0.37	0.047
0.125	0.36	0.047

6°) Multiscale simulations

Methodology

BEGIN OF RUN

The matrix is initialized and the target volume is voxelized.



Linear Interpolation Coefficients C++ Map

The linear interpolation coefficients are calculated after the alpha beta data table

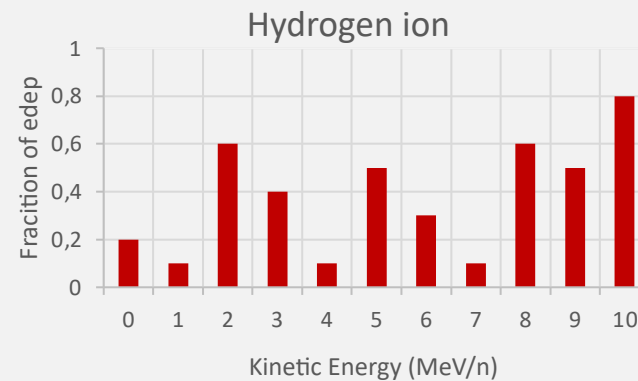
STEPPING ACTION IN VOXEL



Voxel *i*

The information retrieved from each step in each voxel

Deposited Energy C++ Map



The deposited energy is retrieved to estimate the fraction of deposited energy per ion type

Alpha Beta Mix Values C++ Map

$$\alpha_{mix} = \sum f_T a_T \quad \sqrt{\beta_{mix}} = \sum f_T \sqrt{\beta_T}$$

The linear interpolation coefficients are used to calculate the alpha and beta mix values

END OF RUN

Using the stored alpha and beta mix values, the following quantities are estimated per voxel :

RBE
 BIOLOGICAL DOSE
 SURVIVAL FRACTION

OUTPUT

The output file contains the survival fraction, biological dose and RBE per voxel

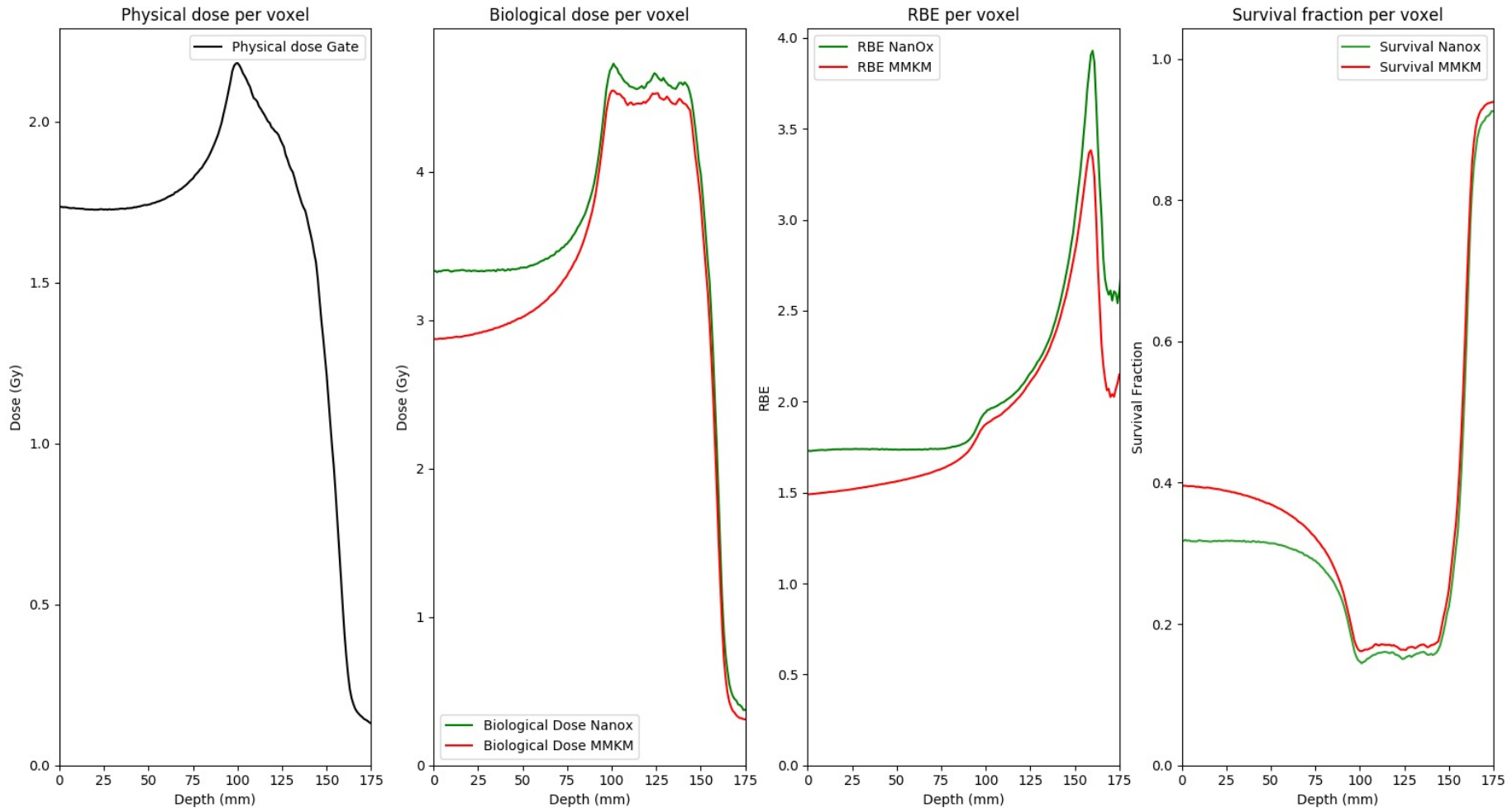
PENCIL BEAM SCANNING
 No post treatment needed

PASSIVE MODULATION
 Python script to combine the output of each mono-energetic peak

6°) Multiscale simulations

Some results

HIMAC LINE
Chiba, Japan



Internship open in 2022 to continue the work in patient CT-scans

7°) Events



GATE training for beginners 23-25 November 2021

<https://cnrsformation.cnrs.fr/gate-training-on-medical-imaging-dosimetry-radiation-therapy?mc=GATE%20Training>

Direction des Relations avec les Entreprises

CNRS FORMATION
ENTREPRISES

Python Data Analysis for GATE simulations 8-10 March 2022

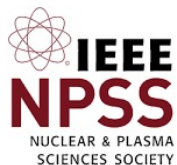
<https://cnrsformation.cnrs.fr/gate-training-on-medical-imaging-dosimetry-radiation-therapy?mc=GATE%20Training>

GATE trainings for master programs

- Server dedicated to training
- Initiated in France this year
- To be extended to any master program



Masters in particle & medical physics (200 students)



GATE workshop 23rd of October 2021

<https://nssmic.ieee.org/2021/program/>

Next GATE scientific meeting

18th of November 2021

Information coming soon